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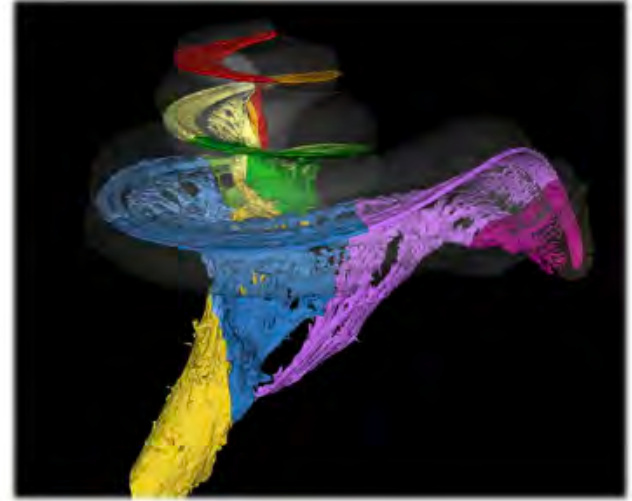
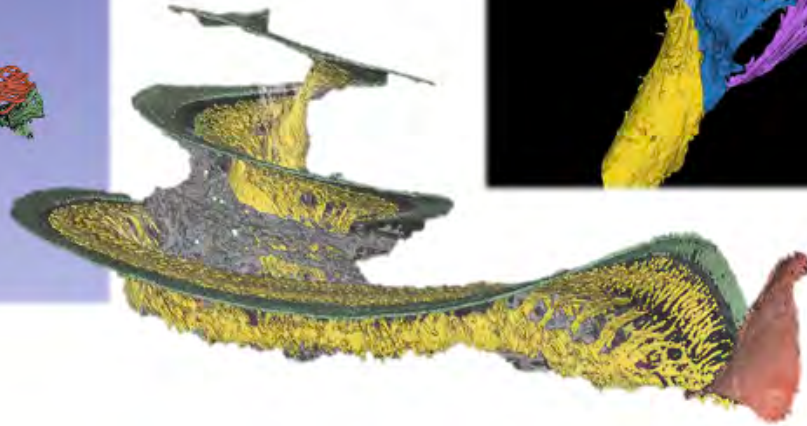
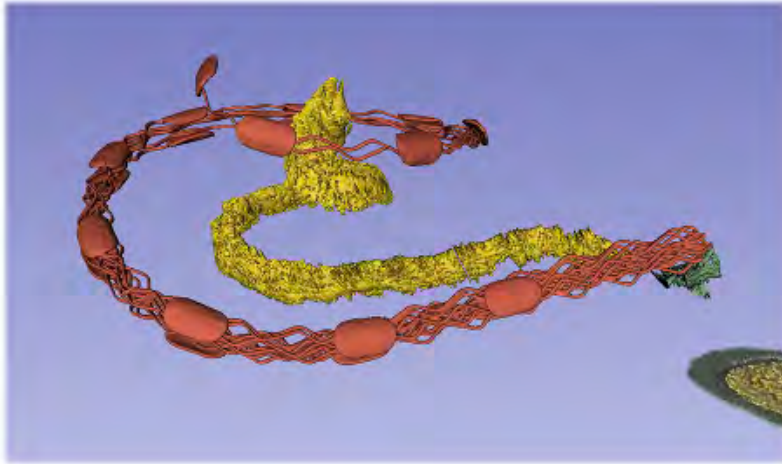
Move over Mickey Mouse™

Turning the tables on what you know about CI sound quality

Josh Stohl, PhD

Director – North American Research Laboratory

MED-EL's key design principles



Images provided by Hanif Ladak and Luke Helpard



MED-EL's key design principles



Atraumatic electrode arrays

Complete cochlear coverage

Natural sound coding



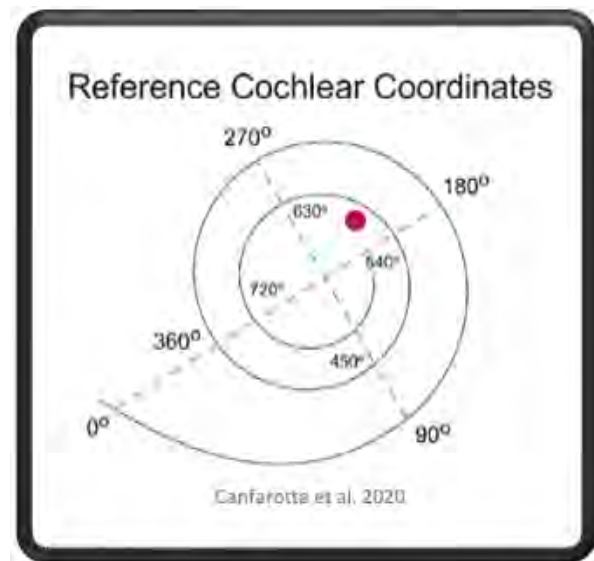
Images provided by Hanif Ladak and Luke Helpard



Voice of the CI

Learning from SSD CI users

- Dorman et al. had single-sided deaf (SSD) cochlear implant (CI) users listen to acoustic simulations of CIs to better understand device sound quality
- 17-year-old patient with 2 years device experience
- FLEX28 with angular insertion depth of 580 degrees
- Programmed with FS4-p
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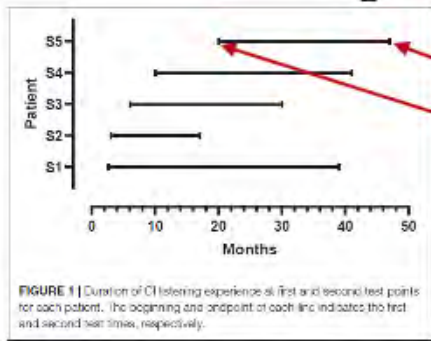


Voice of the CI

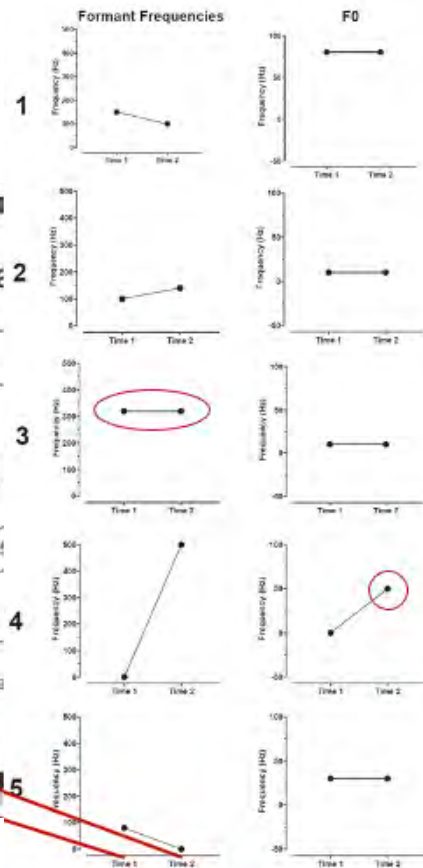
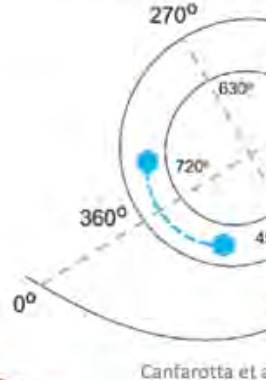
Learning from SSD CI users

TABLE 1 | Selected biographical data for patients.

Subject ID	Age at time of test 1 (years)	Duration deaf (years)	Insertion Depth (degrees)
1	38	1.7	409
2	26	2.7	387
3	49	3.5	419
4	40	0.22	395
5	52	8.2	340



Reference Cochlea: 2



Dorman, M. F., et al. "Upward Shifts in the Internal Representation of Frequency Can Persist Over a 3-Year Period for Cochlear Implant Patients Fit With a Relatively Short Electrode Array." *Front. Hum. Neurosci.* (2022)

Voice of the CI

Learning from SSD CI users

Insertion angles between 340° and 419°

- Upshift in F0 pitch and speech frequencies
- Can persist for years

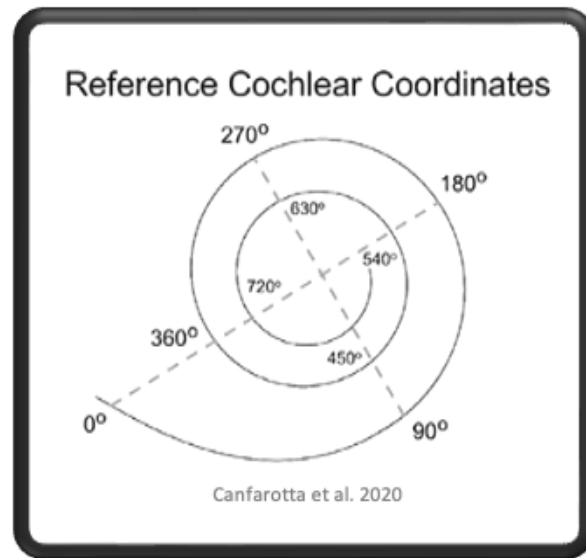
Insertion angles shallower than $\sim 450^\circ$

- Upshift in F0 pitch
- Upshifted speech frequency spectrum

Insertion angles greater than $\sim 450^\circ$

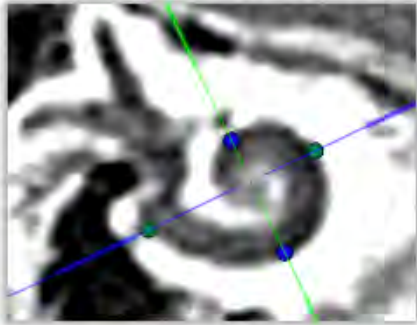
- No upshift in pitch
- No upshift in speech frequencies

Dorman et al.

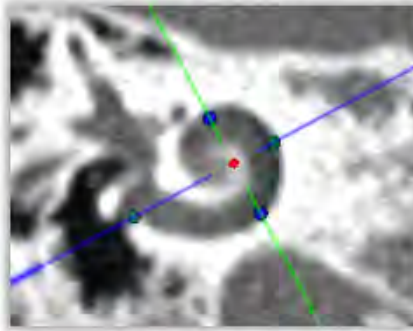


Electrode array + Cochlear duct length

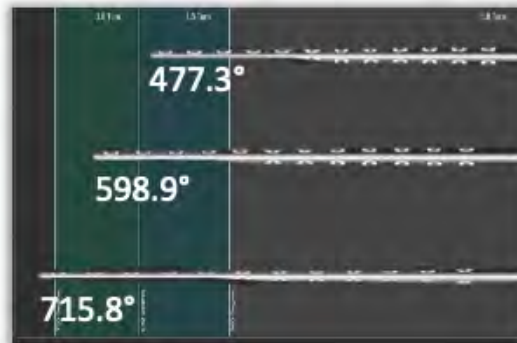
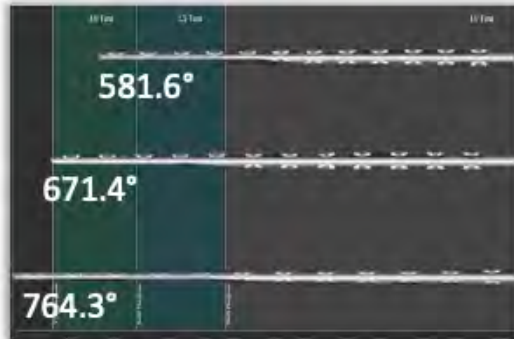
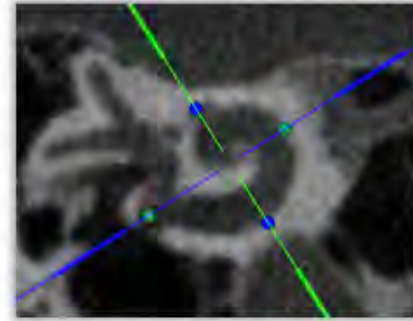
Short CDL
29.79 mm



Average CDL
33.84 mm

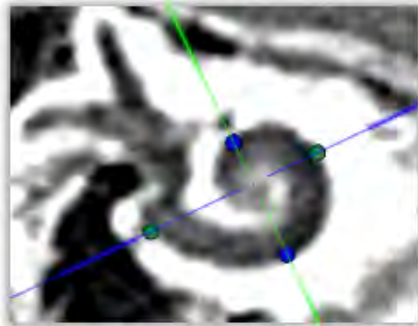


Long CDL
40.27 mm

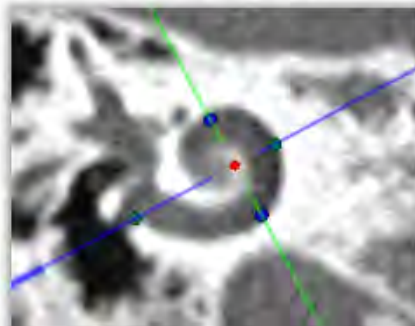


Electrode array + Cochlear duct length

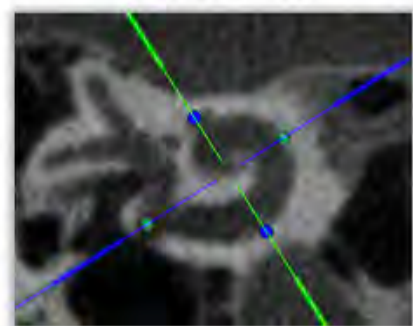
Short CDL
29.79 mm



Average CDL
33.84 mm



Long CDL
40.27 mm



FLEX24

FLEX28

FLEXSoft

OTOPLAN ON DEMAND



Preoperatively assists in choosing the optimal array length based on an individual's unique cochlear duct length (CDL)



MED-EL's key design principles



Atraumatic electrode arrays

A 3D model of a cochlea, showing the spiral structure. A yellow electrode array is shown inserted into the cochlea, with red and orange components visible. The model is set against a light blue background.



Complete cochlear coverage

A 3D model of a cochlea, showing the spiral structure. A yellow electrode array is shown inserted into the cochlea, with red and orange components visible. The model is set against a light blue background.

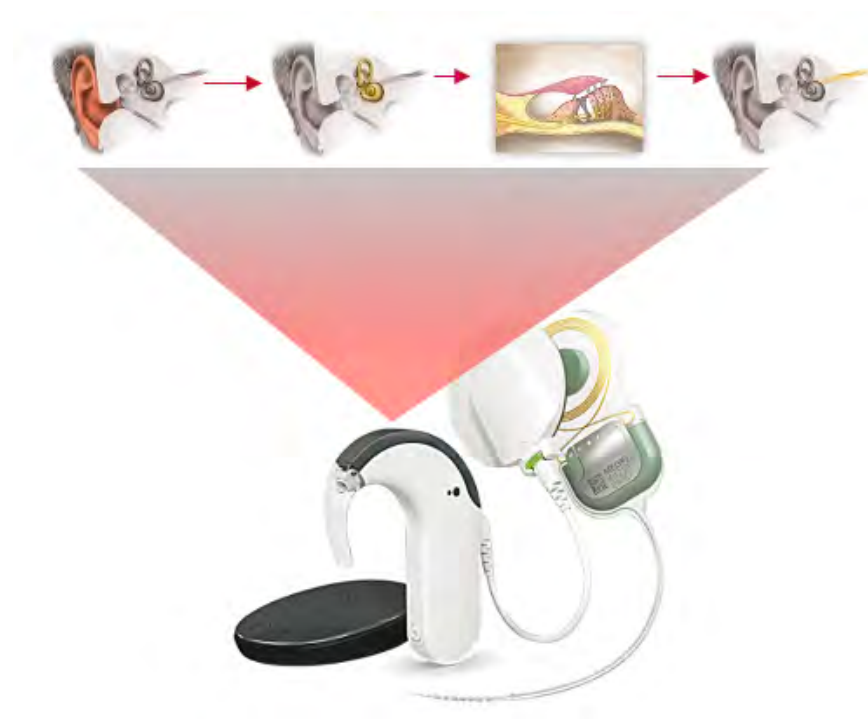
Natural sound coding

Images provided by Hanif Ladak and Luke Helpard



Natural Sound Coding

MED-EL's broad design goal is to mimic the natural auditory system



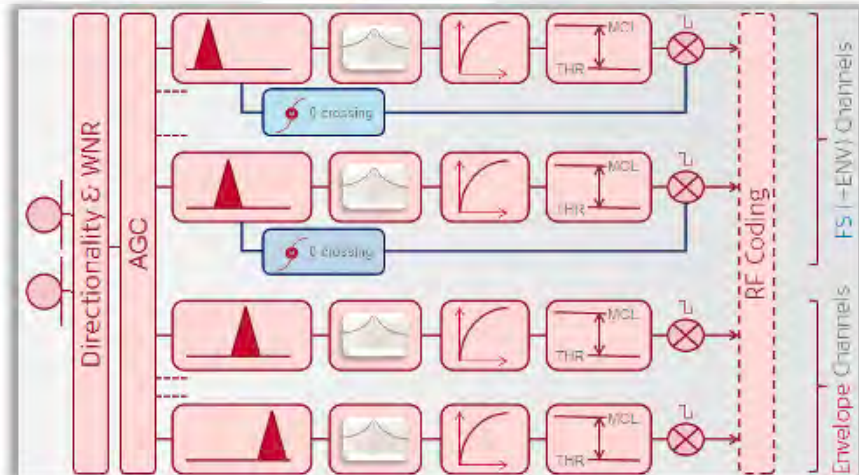
Sound to stimulation

Natural sound coding

Sound →

- Microphone(s)
- Directionality, WNR
- Automatic gain control (AGC)
- Bell-shaped bandpass filters
- Envelope extraction
- Noise reduction
- Zero-crossing detection
- Maplaw compression
- Patient-specific fitting

→ Stimulation



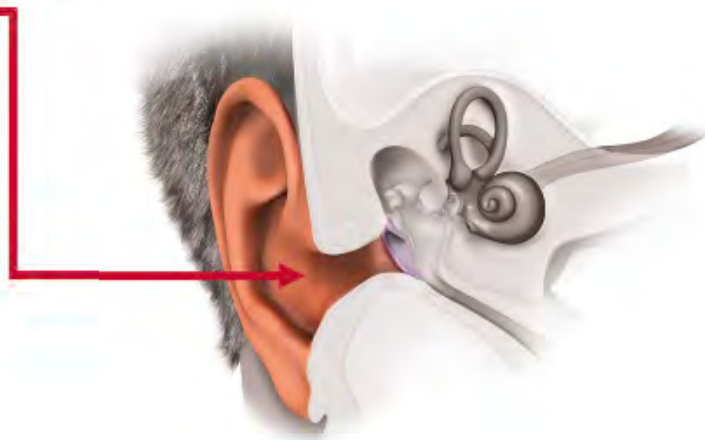
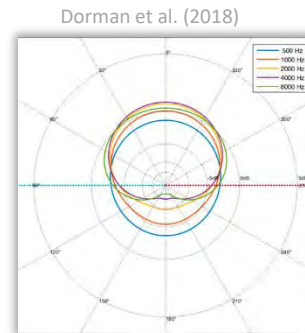
Sound to stimulation

Natural sound coding

Sound →

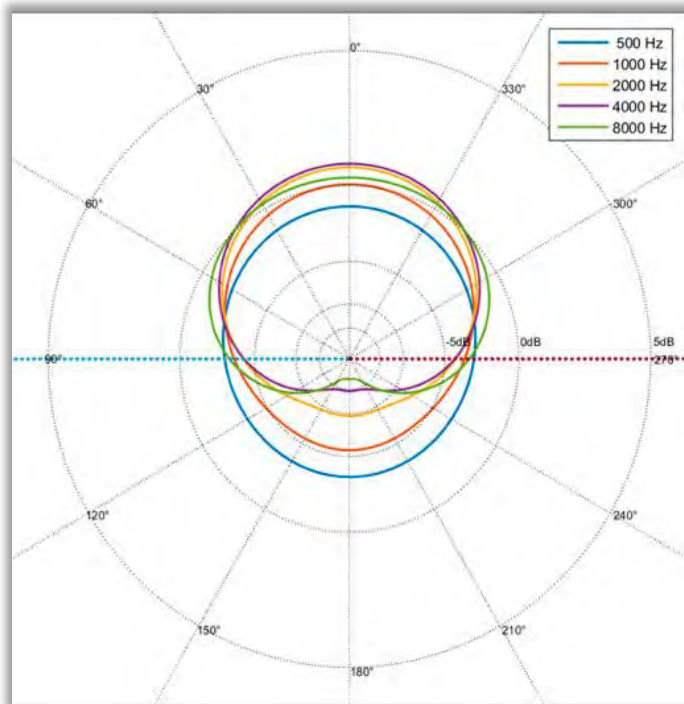
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- Maplaw compression
- Patient-specific fitting

→ Stimulation



Sound to stimulation

Natural sound coding



Dorman et al. (2018)

Emphasizes sounds in front of the listener



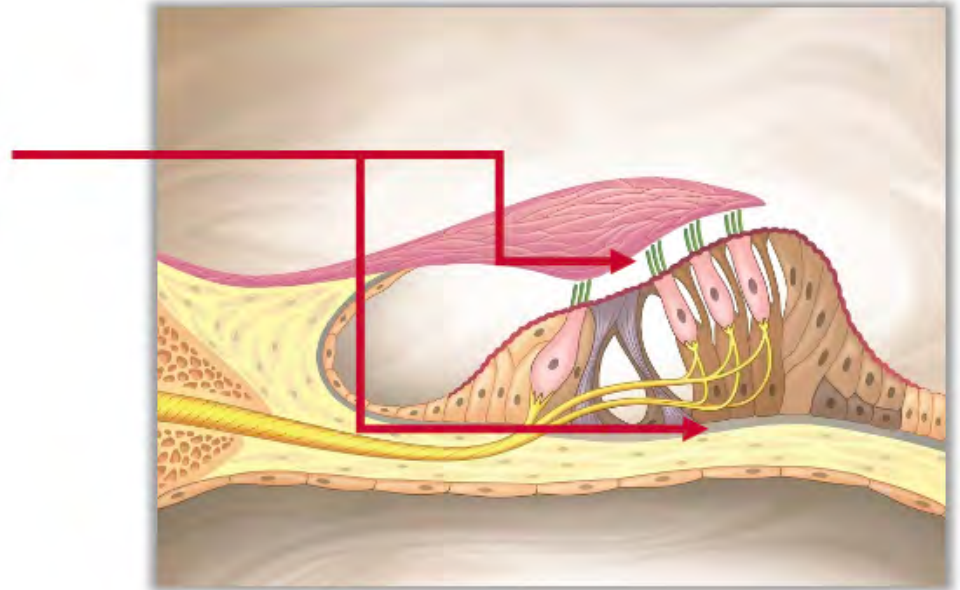
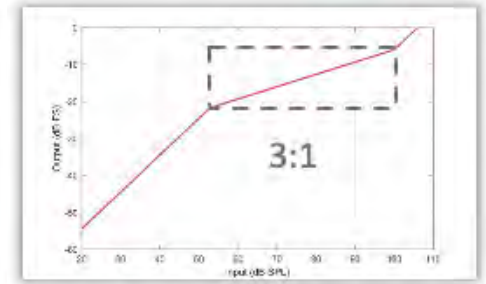
Sound to stimulation

Natural sound coding

Sound →

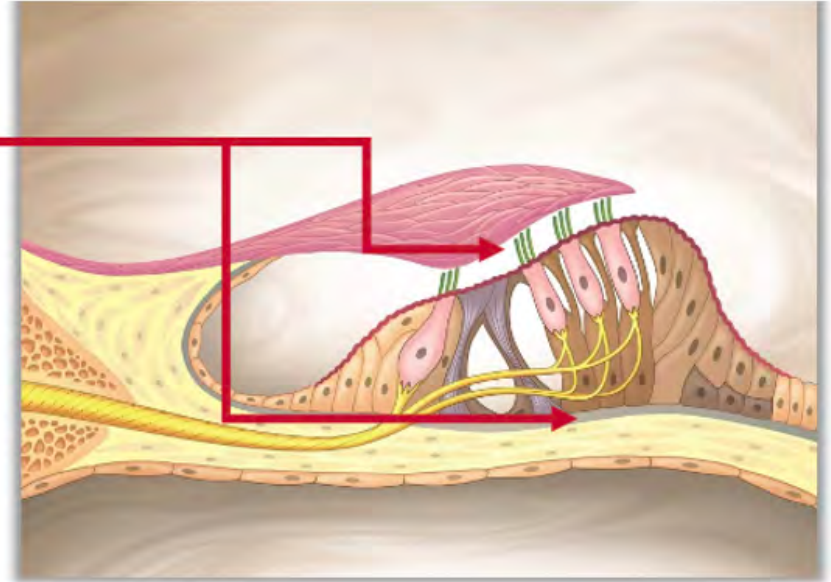
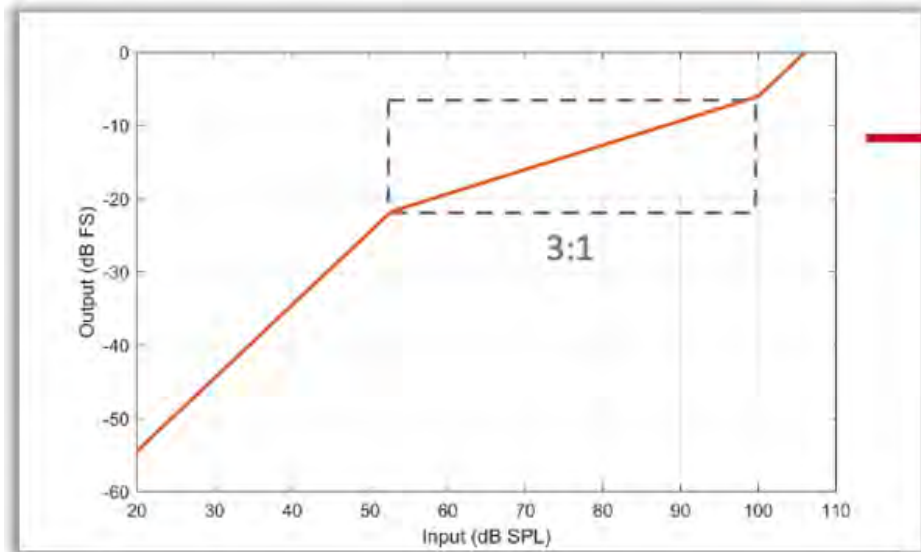
- Microphone(s)
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- Maplaw compression
- Patient-specific fitting

→ Stimulation



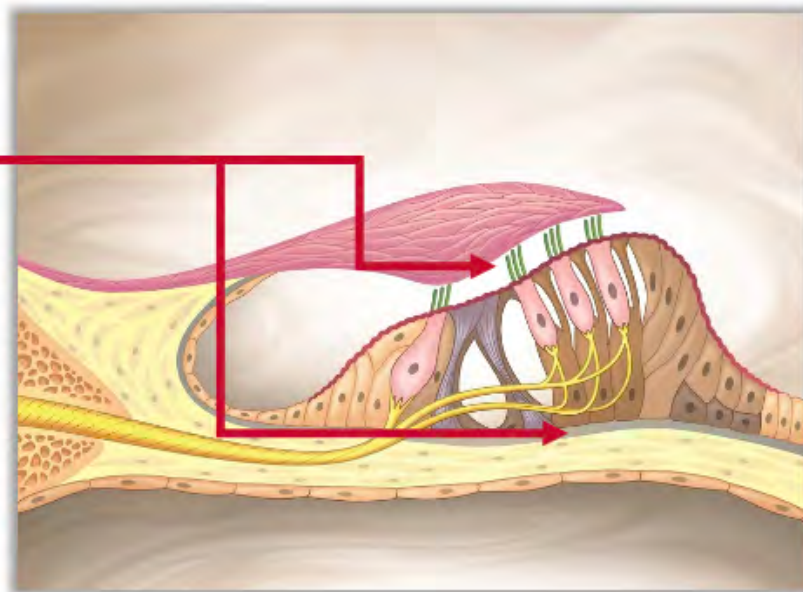
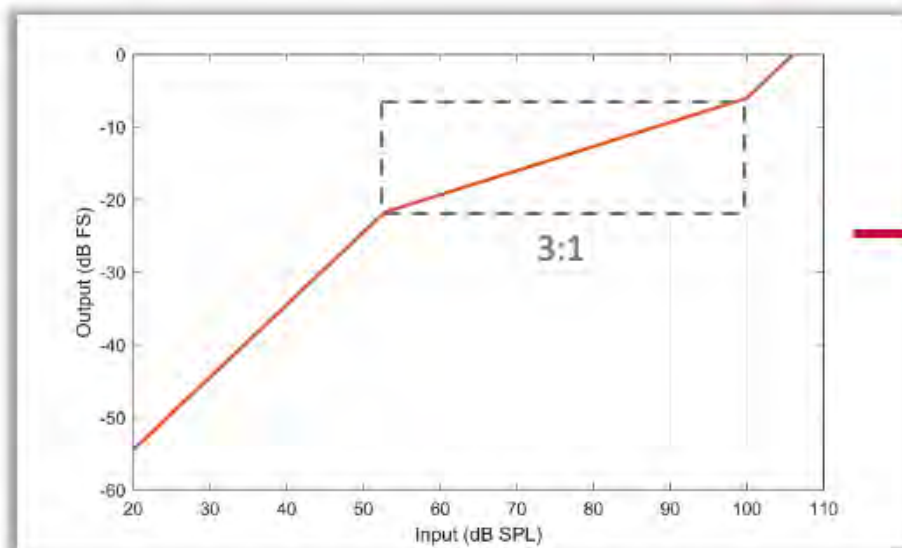
Sound to stimulation

Natural sound coding



Sound to stimulation

Natural sound coding



	250 Hz	500 Hz	1 kHz	2 kHz	4 kHz	8 kHz
Compression ratio (dB/dB)	1.32	2.00	2.91	3.10	2.83	2.44

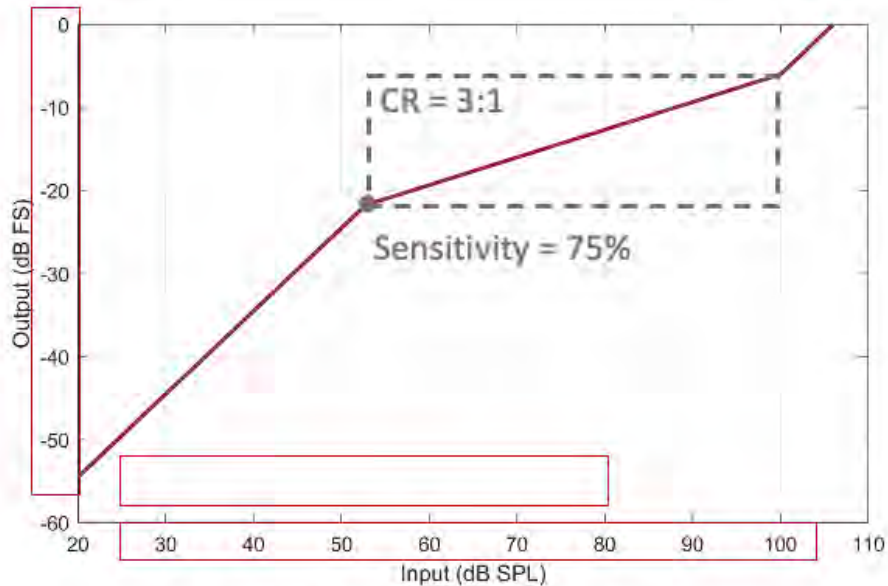
Basilar membrane compression (Plack and Oxenham, 2000)

Automatic gain control (AGC)

Wide input dynamic range



Instantaneous input dynamic range (55 dB)

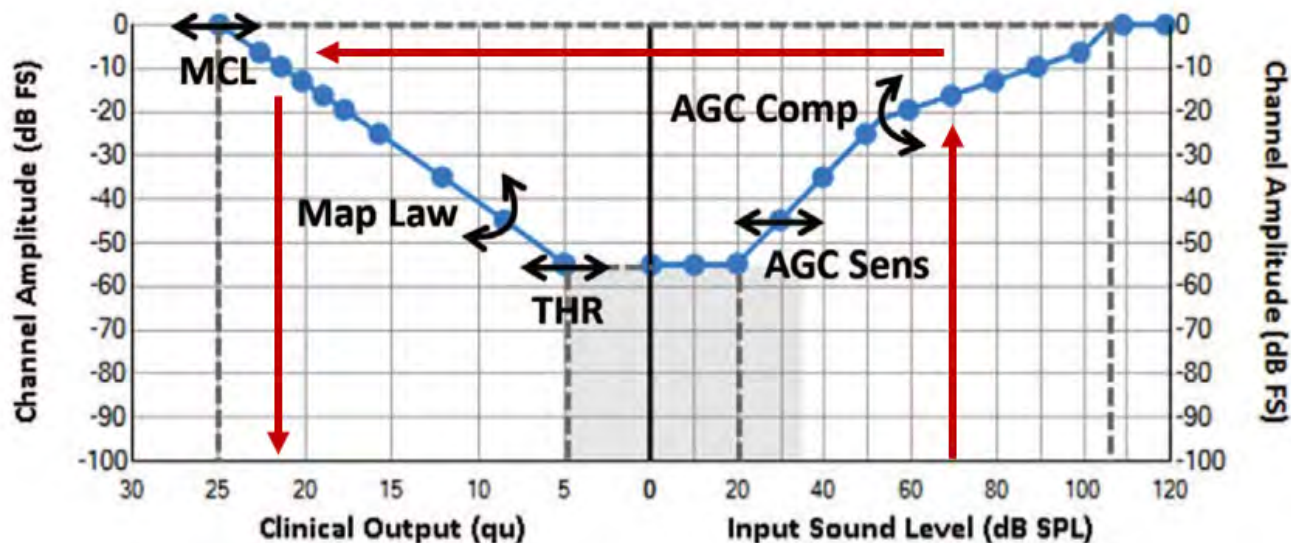


Input dynamic range (~75 dB)



Automatic gain control (AGC)

Comparing CI systems



Vaerenberg B, Govaerts PJ, Stainsby T, Nopp P, Gault A, and Gnansia D,
“A uniform graphical representation of intensity coding in current-generation cochlear implant systems,”
Ear and Hearing, vol. 35, no. 5, pp. 533–543, 2014.

Automatic gain control (AGC)

Comparing CI systems

MED-EL

- Linear up to kneepoint (Sensitivity)
- Natural compression above kneepoint (3:1)

Cochlear

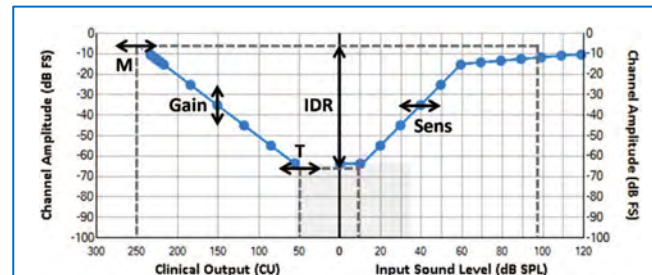
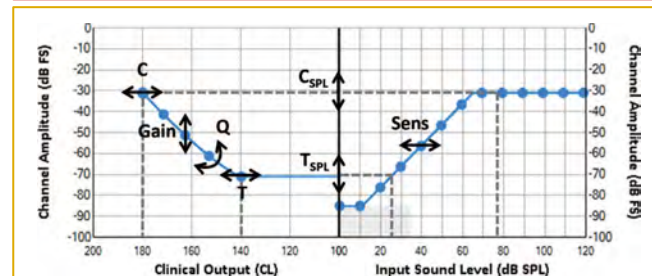
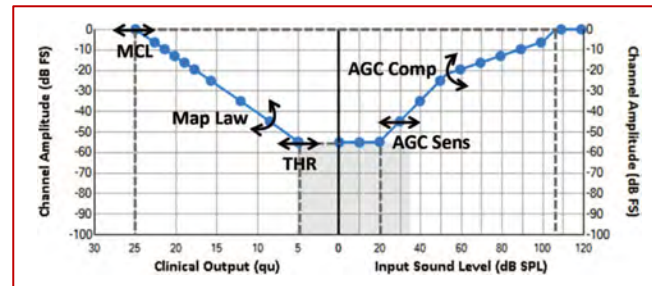
- Linear up to C-SPL
- Infinite compression/limiter at C-SPL (65 dB SPL)

Advanced Bionics

- Linear up to kneepoint (sensitivity)
- Limiting above kneepoint (12:1)

Limiting at medium levels by competitors

- Suggests focus on conversational speech
- May create asymmetric loudness growth when paired with hearing aid, (near-)normal hearing

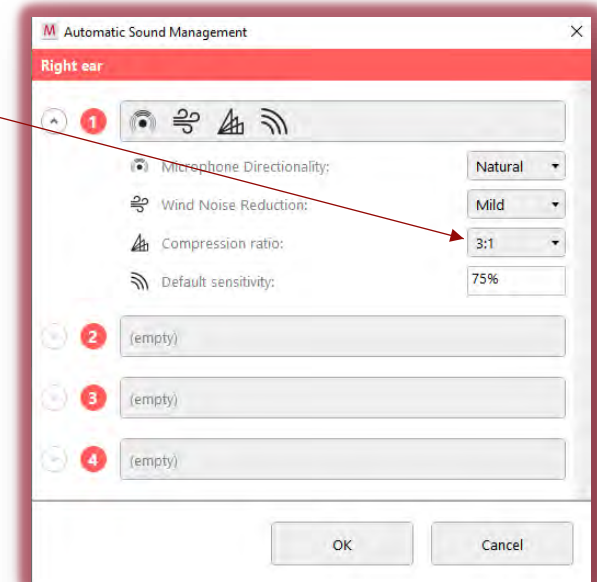


Automatic Gain Control

Compression ratio can be adjusted to match hearing aid

Allows for preferred amplification solution

Matches natural compression by default (SSD)



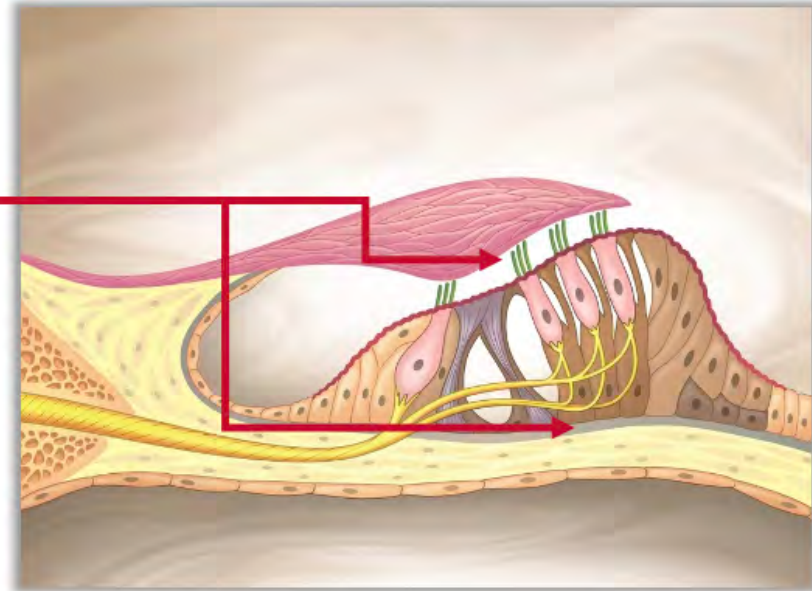
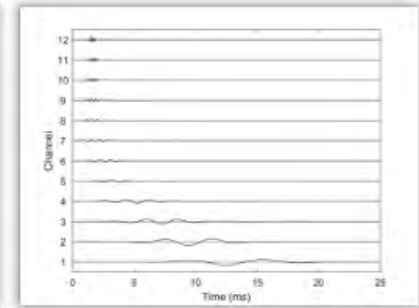
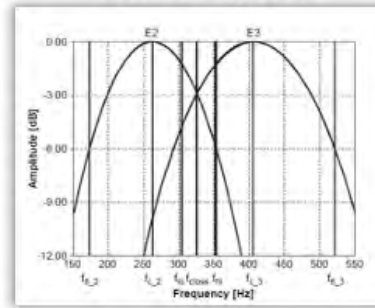
Sound to stimulation

Natural sound coding

Sound →

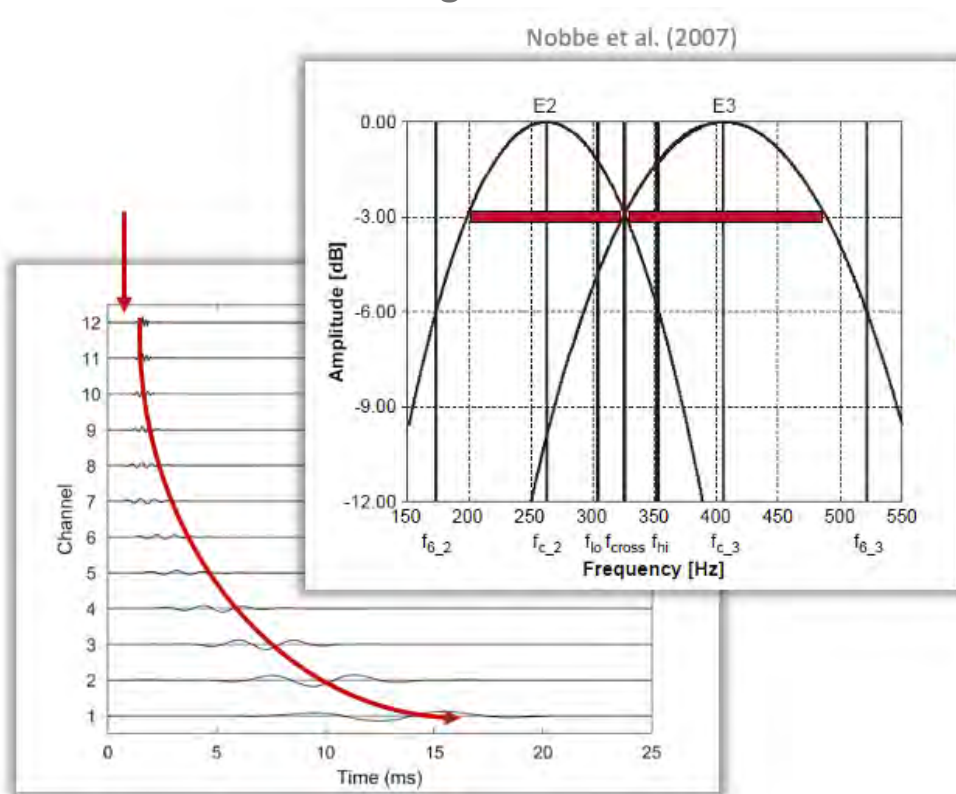
- Microphone(s)
- Directionality, WNR
- Automatic gain control (AGC)
- **Bell-shaped bandpass filters**
- Envelope extraction
- Noise reduction
- Zero-crossing detection
- Maplaw compression
- Patient-specific fitting

→ Stimulation



Sound to stimulation

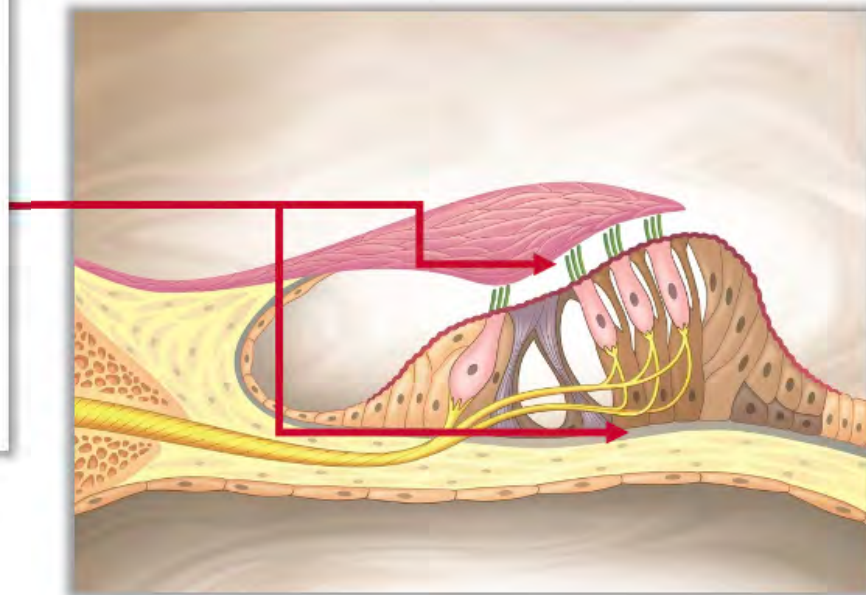
Natural sound coding



Intermediate pitches

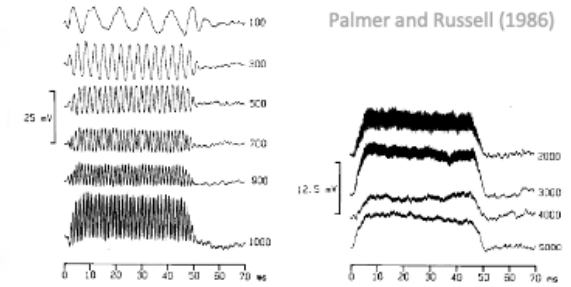
Short processing delay

Mimic traveling wave delays



Sound to stimulation

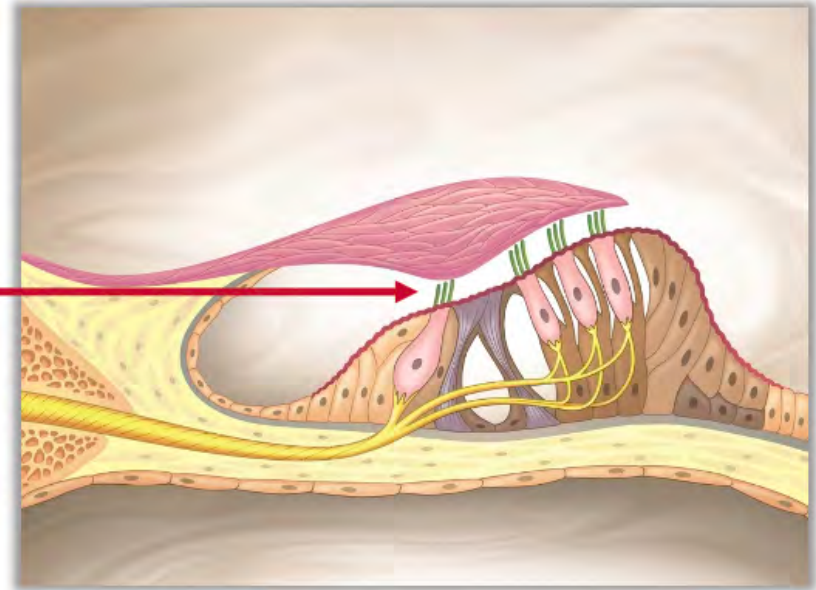
Natural sound coding



Sound →

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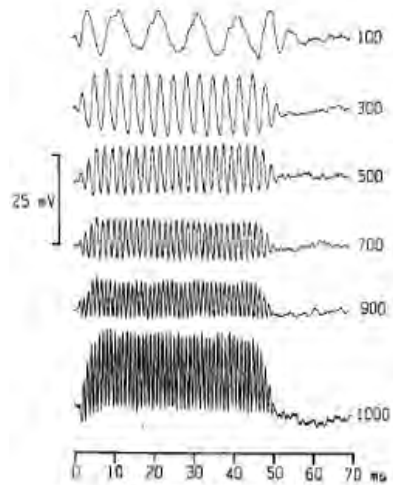
→ Stimulation



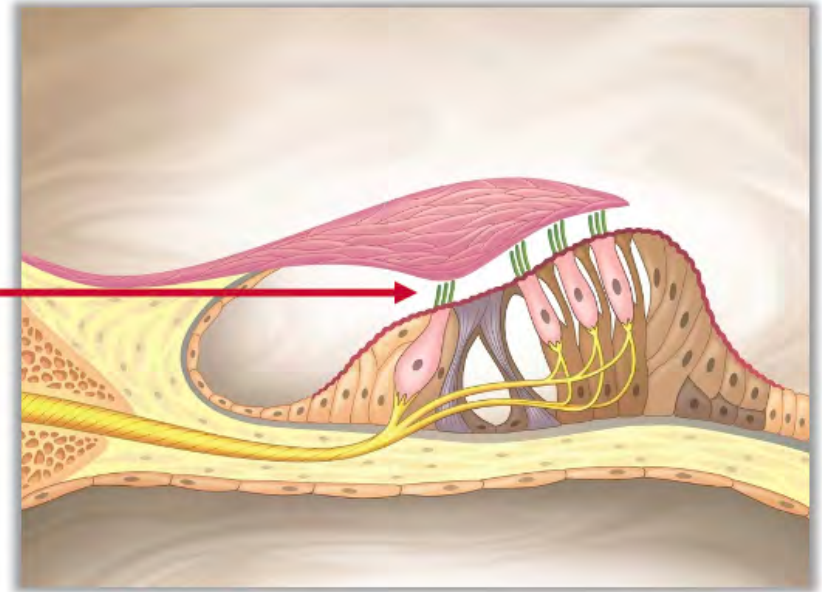
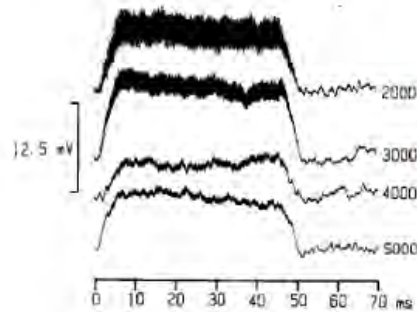
Sound to stimulation

Natural sound coding

Envelope +
Fine structure



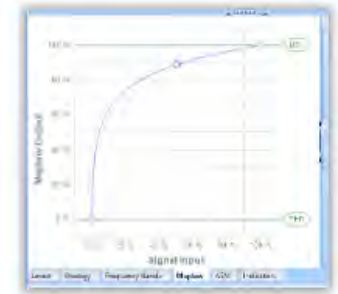
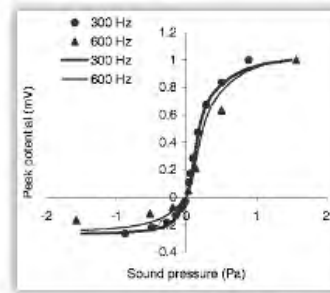
Envelope-only



Palmer and Russell (1986)

Sound to stimulation

Natural sound coding

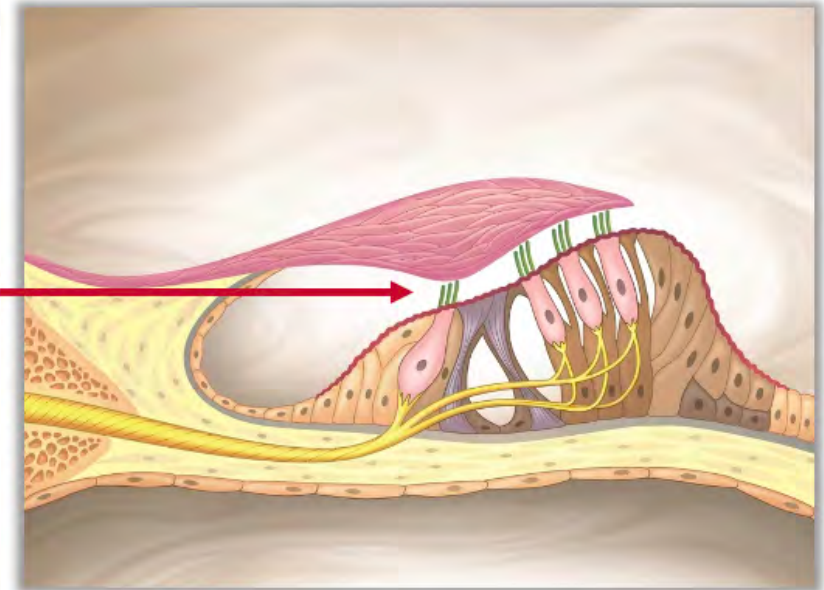


Russell et al. (1986); Lopez-Poveda and Eustaquio-Martin (2006)

Sound →

- Microphone(s)
- Directionality, WNR (BTE)
- Automatic gain control (AGC)
- Bell-shaped bandpass filters
- Envelope extraction
- Noise reduction
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- **Maplaw compression**
- Patient-specific fitting

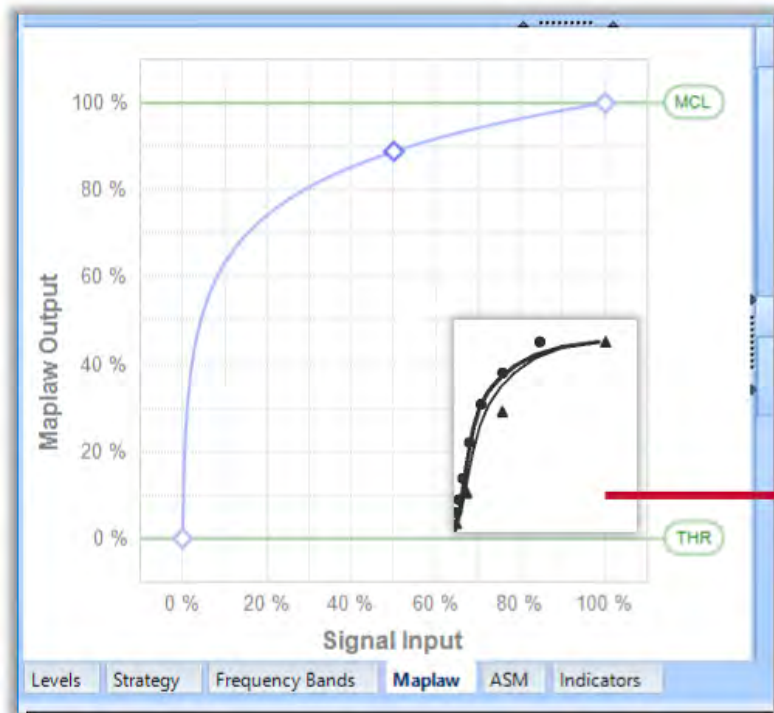
→ Stimulation



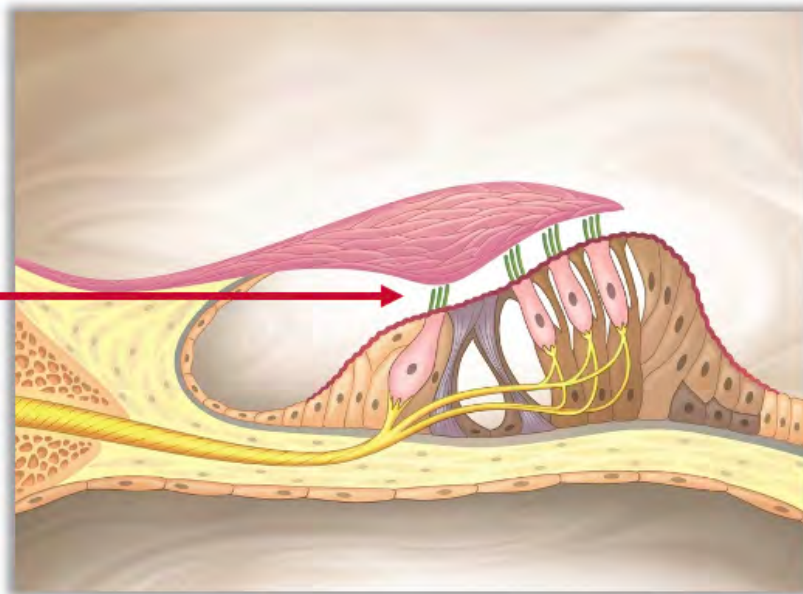
Sound to stimulation

Natural sound coding

Maplaw compression mimics
inner hair cell compression



Russell et al. (1986); Lopez-Poveda and Eustaquio-Martin (2006)

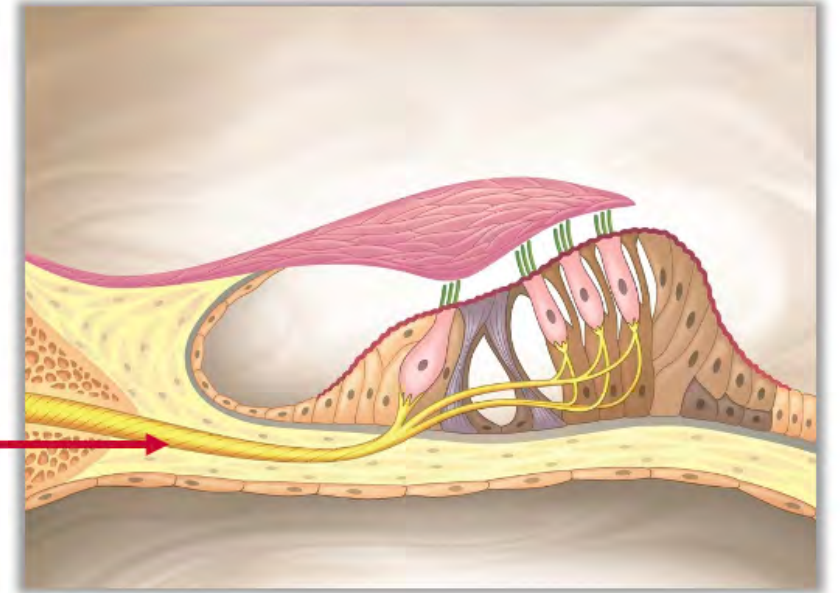


Natural sound coding

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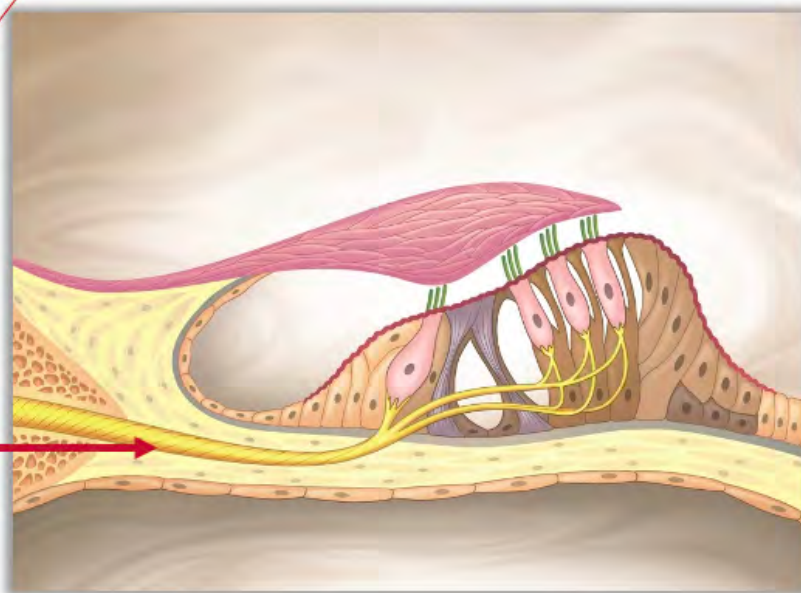
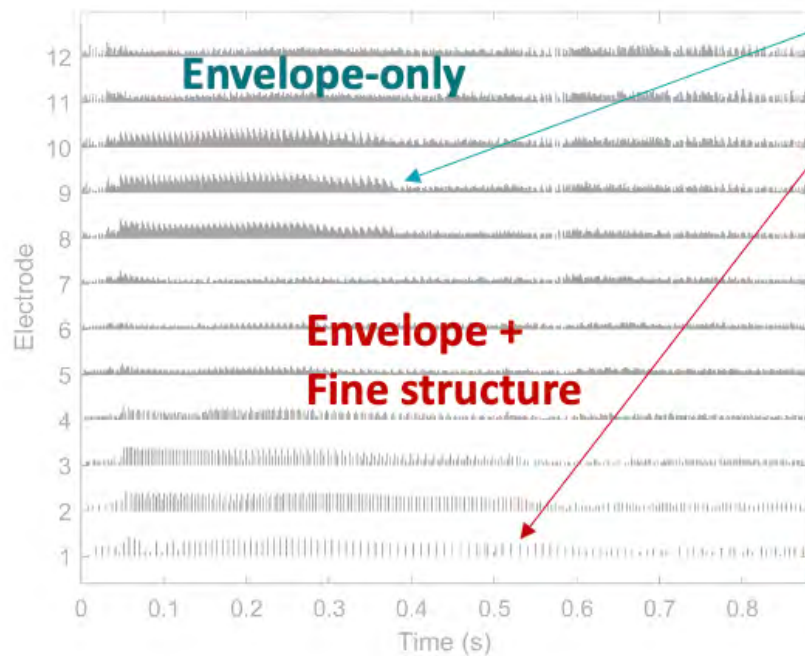
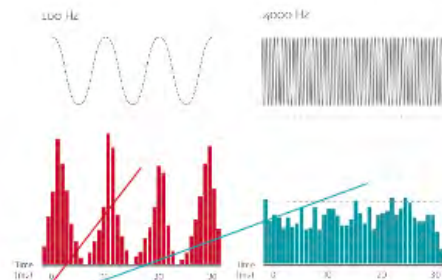
- Patient-specific fitting

→ Stimulation



Sound to stimulation

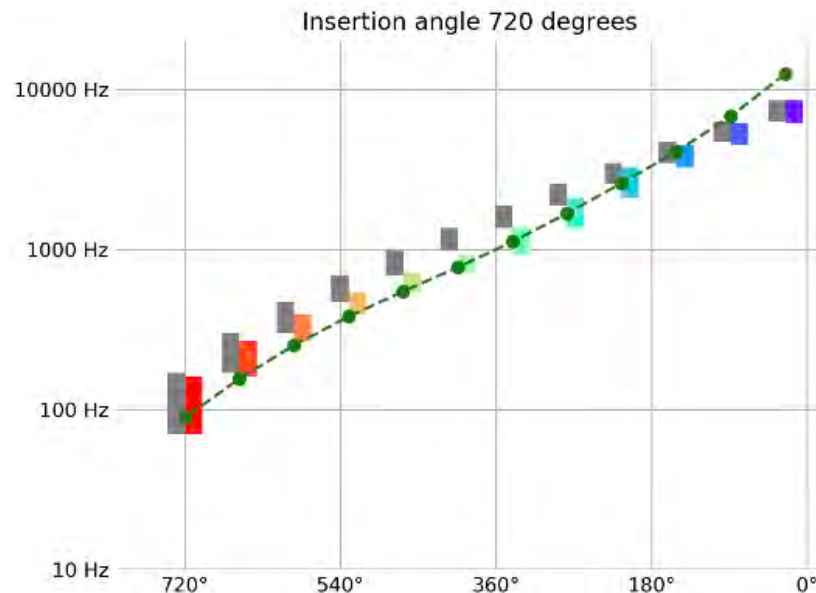
Natural sound coding



Anatomy-Based Fitting (ABF)

ABF is MED-EL's new frequency allocation option that utilizes information from OTOPLAN

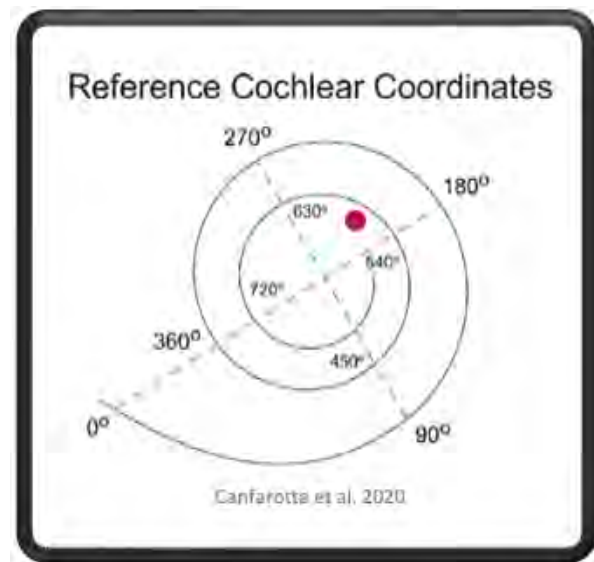
ABF has a goal of aligning processor frequency bands with anatomy-based frequencies associated with electrode contacts to better match natural sound coding



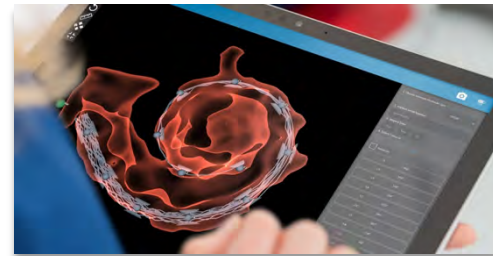
Voice of the CI

Learning from SSD CI users

- Dorman et al. had single-sided deaf (SSD) cochlear implant (CI) users listen to acoustic simulations of CIs to better understand device sound quality
- 17-year-old patient with 2 years device experience
- FLEX28 with angular insertion depth of 580 degrees
- Programmed with FS4-p
- Electrode 1 deactivated to simulate an angular insertion depth of 461 degrees



Summary



Long-standing key design principles:

Atraumatic electrode arrays

Complete cochlear coverage

Natural sound coding

Individualized cochlear implantation:

Pre-planning with OTOPLAN

Post-op frequency fitting with Anatomy-Based Fitting

Closest to Natural Hearing

Move over Mickey Mouse™!

References

- Canfarotta, M. W., et al. (2020). "Frequency-to-Place Mismatch: Characterizing Variability and the Influence on Speech Perception Outcomes in Cochlear Implant Recipients." *Ear Hear* 41(5): 1349-1361.
- Dorman, M. F., et al. (2018). "Speech understanding and sound source localization by cochlear implant listeners using a pinna-effect imitating microphone and an adaptive beamformer." *Am J Audiol* 29(3): 197-205.
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- Lopez-Poveda, E. A. and A. Eustaquio-Martin (2006). "A biophysical model of the inner hair cell: the contribution of potassium currents to peripheral auditory compression." *J Assoc Res Otolaryngol* 7(3): 218-235.
- Nobbe, A., et al. (2007). "Frequency discrimination with sequential or simultaneous stimulation in MED-EL cochlear implants." *Acta Otolaryngol* 127(12): 1266-1272.
- Palmer, A. and I. Russell (1986). "Phase-locking in the cochlear nerve of the guinea-pig and its relation to the receptor potential of inner hair-cells." *Hear Res* 24(1): 1-15.
- Plack, C. J. and A. J. Oxenham (2000). "Basilar-membrane nonlinearity estimated by pulsation threshold." *J Acoust Soc Am* 107(1): 501-507.
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Thank you for listening!